Outline

*Introduction of new class of signals *As an extension of bandlimited signals *Sampling and Reconstruction *Noiseless case *Noisy case * Application ***** Compression of ECG signals *Line-edge extraction

Compression of ECG Signals

Hao et al. (2005)



Approximation Results

MIT/BIH Arrhythmia Database

Data 103



Outline

*Introduction of new class of signals *As an extension of bandlimited signals *Sampling and Reconstruction *Noiseless case *Noisy case * Application *****Compression of ECG signals *Line-edge extraction

Line-Edge Extraction



Navigation by lane-detection

Registraction for super-resolution





Standard Method: Hough Trans.







Preciseness degrades as resolution decreases

Trade-off between sensitivity and preciseness

New Approach: Sampling Theory

* Pixel acquisition process is modeled by spline functions







(Baboulaz et al., 2009)

 $h[m,n] = \langle f(x,y), \psi(x-m)\psi(y-n) \rangle$

Pixel value

Continuous image

Point Spread Function Model By B-spline or E-spline



... + $c_0^{(p)}\beta_P(t) + c_1^{(p)}\beta_P(t-1) + c_2^{(p)}\beta_P(t-2) + \ldots = t^p$

Moment of Image

$$g[n] = \left\langle f(t), \beta_P(t-n) \right\rangle$$
$$\sum_{n=-\infty}^{\infty} c_n^{(p)} g[n] = \sum_{n=-\infty}^{\infty} c_n^{(p)} \left\langle f(t), \beta_P(t-n) \right\rangle$$

$$= \left\langle f(t), \sum_{n=-\infty}^{\infty} c_n^{(p)} \beta_P(t-n) \right\rangle$$

 $= \left\langle f(t), t^p \right\rangle$

$$=\int_{-\infty}^{\infty}f(t)t^{p}\,dt$$

E-spline of Degree 1



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B-Spline & tri. E-Spline

B-Spline of Degree 1

Trigonometric E-Spline

$$\beta_{1}(t) = \begin{cases} 1+t & (-1 < t < 0) \\ 1-t & (0 < t < 1) \\ 0 & (|t| > 0) \end{cases}$$

 $\beta_{\vec{\alpha}}(t) = \begin{cases} \sin \omega_0 (1+t) / \omega_0 & (-1 < t < 0) \\ \sin \omega_0 (1-t) / \omega_0 & (0 < t < 1) \\ 0 & (|t| > 0) \end{cases}$





Sinusoid Reconstruction by Trigonometric E-spline



 $\dots + c_0^{(\alpha_p)} \beta_{\vec{\alpha}}(t) + c_1^{(\alpha_p)} \beta_{\vec{\alpha}}(t-1) + c_2^{(\alpha_p)} \beta_{\vec{\alpha}}(t-2) + \dots = e^{\alpha_p t}$

Exponential Moment of Image

$$g[n] = \langle f(t), \beta_{p}(t-n) \rangle$$

$$\sum_{n=-\infty}^{\infty} c_{n}^{(p)} g[n] = \sum_{n=-\infty}^{\infty} c_{n}^{(p)} \langle f(t), \beta_{p}(t-n) \rangle$$

$$= \langle f(t), \sum_{n=-\infty}^{\infty} c_{n}^{(p)} \beta_{p}(t-n) \rangle$$

$$= \langle f(t), e^{\alpha_{p}t} \rangle$$

$$= \int_{-\infty}^{\infty} f(t) e^{\alpha_{p}t} dt$$

Procedure for Edge Extarction

(Baboulaz et al., 2009, Hirabayashi et al., 2010)



Extraction of Local Area of 8*8

For all detected pixels by Canny detector, we repeat line-edge extraction procedure. To do so, we extract 8*8 local image around the focusing pixel.



Step Line-Edge Representation

$$f(x, y) = \lambda u(-x\sin\theta + y\cos\theta + \gamma\sin\theta)$$
$$u(t) = \begin{cases} 0 & (t < 0) \\ 1 & (t \ge 0) \end{cases}$$

Step Line-Edge Representation

$$f(x, y) = \lambda u(-x\sin\theta + y\cos\theta + \gamma\sin\theta)$$
$$u(t) = \begin{cases} 0 & (t < 0) \\ 1 & (t \ge 0) \end{cases}$$

 $g[m,n] = \langle f(x,y), \psi(x-m)\psi(y-n) \rangle + \varepsilon[m,n]$

 $\psi(t)$: Trigonometric E-spline $\varepsilon[m,n]$: Additive noise

Step 1: Differentiated Samples



Differentiated Sample & Derivative of Continuous Image

$$\begin{aligned} d_{H}[m,n] &= g[m+1,n] - g[m,n] \\ &= \left\langle \frac{\partial f(x,y)}{\partial x}, \psi_{+}(x-m)\psi(y-n) \right\rangle \ \text{(15)} \\ &\psi_{+}(t) = (\psi * \beta_{\alpha_{2}})(t-0.5), \\ &\beta_{\alpha_{2}}(t) = \left\{ \begin{array}{c} 1 & (|t| < 0.5) \\ 0 & (|t| \ge 0.5) \end{array} \right. \end{aligned}$$
Cf.

$$g[m,n] = \langle f(x,y), \psi(x-m)\psi(y-n) \rangle$$

Proof

Let $\Phi(t) = \int \psi(t) dt$. Then, it follows that

$$\psi_{+}(t) = \int_{-\infty}^{\infty} \beta_{\alpha_{2}}(t')\psi(t-0.5-t')dt'$$

=
$$\int_{-0.5}^{0.5} \psi(t-t')dt' = \Phi(t) - \Phi(t-1).$$

Differentiating both sides of this equation yields

$$\frac{d}{dt}\psi_+(t) = \psi(t) - \psi(t-1).$$

Hence, it follows that

$$d_H[m,n] = \langle f(x,y), \{\psi(x-m-1) - \psi(x-m)\}\psi(y-n)\rangle$$

$$= \left\langle f(x,y), \left\{-\frac{d}{dt}\psi_{+}(x-m)\right\}\psi(y-n)\right\rangle$$
$$= -\int_{-\infty}^{\infty}\int_{-\infty}^{\infty}f(x,y)\left\{\frac{d}{dx}\psi_{+}(x-m)\right\}\psi(y-n)dxdy$$
$$= \int_{-\infty}^{\infty}\int_{-\infty}^{\infty}\frac{\partial f(x,y)}{\partial x}\psi_{+}(x-m)\psi(y-n)dxdy$$
$$= \left\langle\frac{\partial f(x,y)}{\partial x}, \psi_{+}(x-m)\psi(y-n)\right\rangle,$$

which implies (15). Equation (16) can be shown similarly. \blacksquare



$$\tau_{n,p}^{(H)} = \lambda \mu_{n,p}^{(H)}(\theta, \gamma)$$

$$\mu_{n,p}^{(H)}(\theta,\gamma) = -\operatorname{sgn}(\sin\theta)e^{\alpha_p(\gamma + \frac{n}{\tan\theta} - \frac{1}{2})}\Psi(\frac{\alpha_p}{\tan\theta}) \quad (21)$$

$$\tau_{m,p}^{(V)} = \lambda \mu_{m,p}^{(V)}(\theta, \gamma)$$

$$\mu_{m,p}^{(V)}(\theta, \gamma) = \operatorname{sgn}(\cos \theta) e^{\alpha_p \{-(\gamma - m) \tan \theta - \frac{1}{2}\}} \Psi(\alpha_p \tan \theta)$$

$$\Psi(s) = \int_{-\infty}^{\infty} \psi(t) e^{st} dt \qquad \operatorname{sgn}(t) = \begin{cases} 1 & (t > 0), \\ 0 & (t = 0), \\ -1 & (t < 0) \end{cases}$$

Proof

Proof: Because of (12), we have

$$\frac{\partial f(x,y)}{\partial x} = -\lambda \delta(-x\sin\theta + y\cos\theta + \gamma\sin\theta)\sin\theta,$$

where $\delta(t)$ is Dirac's delta function. Substituting this relation and (15) into (17) yields

$$\tau_{n,p}^{(H)} = \begin{cases} -\lambda e^{\alpha_p (\gamma + n/\tan\theta - \frac{1}{2})} \Psi(\alpha_p/\tan\theta) & (\sin\theta > 0), \\ 0 & (\sin\theta = 0), \\ \lambda e^{\alpha_p (\gamma + n/\tan\theta - \frac{1}{2})} \Psi(\alpha_p/\tan\theta) & (\sin\theta < 0), \end{cases}$$

which are combined into (21).

Step 2: Product-Sum (cnt'd)

Horizontally p = 0 I $n = -1 \begin{pmatrix} \tau_{-1,0}^{(H)} & \tau_{-1,1}^{(H)} \\ \tau_{0,0}^{(H)} & \tau_{0,1}^{(H)} \\ \tau_{1,0}^{(H)} & \tau_{1,1}^{(H)} \end{pmatrix}$

Vertically

 $m = -1 \begin{pmatrix} \tau_{-1,0}^{(V)} & \tau_{-1,1}^{(V)} \\ \tau_{0,0}^{(V)} & \tau_{0,1}^{(V)} \\ \tau_{1,0}^{(V)} & \tau_{1,1}^{(V)} \end{pmatrix}$ $au_{0,2}^{(V)}$

 $\tau^{(H)}_{-1,2}$

 $au_{0,2}^{(ar{H})} \ au_{1,2}^{(H)}$

Criterion for Param. Estimation $J_o(\theta, \gamma, \lambda) = \|\lambda \boldsymbol{\mu}(\theta, \gamma) - \boldsymbol{\tau}\|^2$ $\boldsymbol{\mu}(\theta, \gamma) = \begin{pmatrix} \mu_{-1,0}^{(H)}(\theta, \gamma) \\ \mu_{-1,1}^{(H)}(\theta, \gamma) \\ \mu_{-1,2}^{(H)}(\theta, \gamma) \\ \mu_{0,0}^{(H)}(\theta, \gamma) \\ \vdots \\ \mu_{0,2}^{(V)}(\theta, \gamma) \\ \mu_{1,0}^{(V)}(\theta, \gamma) \\ \mu_{1,1}^{(V)}(\theta, \gamma) \\ \mu_{1,2}^{(V)}(\theta, \gamma) \end{pmatrix} \quad \boldsymbol{\tau} = \begin{pmatrix} \tau_{-1,0}^{(H)} \\ \tau_{-1,1}^{(H)} \\ \tau_{-1,2}^{(H)} \\ \tau_{0,0}^{(H)} \\ \tau_{0,1}^{(H)} \\ \tau_{0,1}^{(V)} \\ \tau_{1,1}^{(V)} \\ \tau_{1,2}^{(V)} \end{pmatrix}$

Optimization in Terms of λ

For fixed θ, γ $J_{o}(\theta, \gamma, \lambda) = \|\mu(\theta, \gamma)\|^{2} \left(\lambda - \frac{\langle \tau, \mu(\theta, \gamma) \rangle}{\|\mu(\theta, \gamma)\|^{2}}\right)^{2} - \frac{\{\langle \tau, \mu(\theta, \gamma) \rangle\}^{2}}{\|\mu(\theta, \gamma)\|^{2}} + \|\tau\|^{2}$ $\geq \|\tau\|^{2} \left[1 - \frac{\{\langle \tau, \mu(\theta, \gamma) \rangle\}^{2}}{\|\tau\|^{2}\|\mu(\theta, \gamma)\|^{2}}\right].$

$$J(\boldsymbol{\theta}, \boldsymbol{\gamma}) = \frac{\{\langle \boldsymbol{\tau}, \boldsymbol{\mu}(\boldsymbol{\theta}, \boldsymbol{\gamma}) \rangle\}^2}{\|\boldsymbol{\tau}\|^2 \|\boldsymbol{\mu}(\boldsymbol{\theta}, \boldsymbol{\gamma})\|^2}$$





Simulation Results

Panasonic Lumix DMC-GF2 (focal length14mm, F2, 1/60s, ISO200)



Super-Resolution

Panasonic Lumix DMC-GF2 (focal length 14mm, F2, 1/60s, ISO200)

Line-edge extraction results





Matching by RANSAC algorithm



Super-resolved from 16 images

Super-Resolution





Super-resolved from 16 images



Summary

- Sampling signals with finite rate of innovation
 Rate of innovation is defined by the number of unknown parameters.
 - •The main signal is the stream of Diracs.
 - •Signal is sampled through the filter
 - •Reconstruction is done by annihilating filter for noiseless case while optimization technique is used for noisy case.
- Applications
 - •Compressive sampling for ECG signals
 - •Step line-edge extraction

Reference

- M. Vetterli, P. Marziliano, and T. Blu, "Sampling signals with finite rate of innovation," IEEE Trans. Signal Processing, vol. 50, no. 6, pp. 1417–1428, June 2002.
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